

## BIOCHEMICAL REACTION CARTRIDGE

### FIELD OF THE INVENTION AND RELATED ART

The present invention relates to biochemical  
5 reaction cartridge used to be incorporated in an  
apparatus for analyzing cell, microorganism,  
chromosome, nuclei acid, etc., in a specimen by  
utilizing a biochemical reaction such as antigen-  
antibody reaction or nucleic acid hybridization.

10 Most of analyzers for analyzing specimens  
such as blood uses an immunological procedure  
utilizing antigen-antibody reaction or a procedure  
utilizing nuclei acid hybridization. For example,  
protein or single-stranded nucleic acid, such as  
15 antibody or antigen, which specifically connects with  
a material or substance to be detected, is used as a  
probe and is fixed on a surface of solid phase, such  
as fine particles, beads or a glass plate, thus  
effecting antigen-antibody reaction or nuclei acid  
20 hybridization. Then, for example, an antigen-antibody  
compound or double-stranded nucleic acid is detected  
by a labeled antigen or labeled nucleic acid, which  
causes a specific interaction such that a labeled  
material having a high detection sensitivity, such as  
25 an enzyme, a fluorescent material or a luminescent  
material, is supported, thus effecting detection of  
presence or absence of the material to be detected or

quantitative determination the detected material.

As an extension of these technologies, e.g.,  
U.S. Patent No. 5,445,934 has disclosed a so-called  
DNA (deoxyribonucleic acid) array wherein a large  
5 number of DNA probes having mutually different base  
sequences are arranged on a substrate in array form.

Further, Anal. Biochem., 270(1), pp. 103 -  
111 (1999) has disclosed a process for preparing a  
protein array, like the DNA array, such that various  
10 species of proteins are arranged on a membrane filter.  
By using these DNA and protein arrays and the like, it  
has become possible to effect a test on a large number  
of items at the same time.

Further, in various methods of specimen  
15 analysis, in order to realize alleviation of  
contamination by specimen, promotion of reaction  
efficiency, reduction in apparatus size, and  
facilitation of operation, there have been also  
proposed disposable biochemical reaction cartridges in  
20 which a necessary reaction is performed in the  
cartridge. For example, Japanese Laid-Open Patent  
Application (JP-A) (Tokuhyo) Hei 11-509094 has  
disclosed a biochemical reaction cartridge, including  
DNA array, in which a plurality of chambers are  
25 disposed and a solution is moved by a differential  
pressure so as to permit a reaction such as  
extraction, amplification or hybridization of DNA in a

specimen within the cartridge.

As a method of supplying a reagent with respect to the biochemical reaction cartridge, JP-A 2000-266759 has disclosed that a reagent is supplied  
5 from an external reagent bottle to a disposable analysis cassette. Further, JP-A (Tokuhyo) Hei 11-505094 has disclosed that a reagent is incorporated in a chamber in advance.

However, in the case of externally supplying  
10 the reagent, a plurality of reagents must be prepared separately from the biochemical reaction cartridge, and if the number of test items is large, the number of necessary reagents is also increased. As a result, replenishment of the reagents becomes complicated and  
15 there is a possibility of erroneously selecting the species of the reagents. Further, in the case of incorporating the reagent in the chamber of biochemical reaction cartridge, there is a possibility such that a reaction different from an intended  
20 reaction is caused to occur by flowing of the reagent in the chamber into a passage or another chamber due to an environmental change at the time of storage or conveyance or vibration during conveyance.

## 25 SUMMARY OF THE INVENTION

An object of the present invention is to provide a biochemical reaction cartridge, having

solved the above described problems, which eliminates the inconvenience of replenishment of a reagent and erroneous selection of the species of reagent and causes no flowing of the reagent in a chamber into a passage or vibration at the time of storage or conveyance.

Another object of the present invention is to provide a biochemical reaction apparatus for effecting a biochemical reaction by using the biochemical reaction cartridge.

According to the present invention, there is provided a biochemical reaction cartridge, comprising:  
a reaction portion, comprising a chamber and a passage, for effecting a biochemical reaction, and  
a solution storage portion, which is isolated or separated from the reaction portion, for storing a solution in a position corresponding to the chamber,  
wherein the cartridge is provided with a penetrable partition member disposed between the solution storage portion and the reaction portion so as to move the solution from the solution storage portion to the chamber of the reaction portion.

These and other objects, features and advantages of the present invention will become more apparent upon a consideration of the following description of the preferred embodiments of the present invention taken in conjunction with the

accompanying drawings.

BRIEF DESCRIPTION OF THE DRAWINGS

Figure 1 is a perspective view of an  
5 embodiment of the biochemical reaction cartridge  
according to the present invention.

Figure 2 is a plan view of a solution storage  
portion.

Figure 3 is a partial sectional view of the  
10 biochemical reaction cartridge at the time of storage.

Figure 4 is a partial sectional view of the  
biochemical reaction cartridge in such a state that a  
valve stem (rod) is pressed by first-stage pushing.

Figure 5 is a partial sectional view of the  
15 biochemical reaction cartridge in such a state that a  
valve stem is pressed by second-state pushing.

Figure 6 is a plan view of a reaction  
portion.

Figure 7 is a block diagram of a treatment  
20 apparatus for controlling movement of a solution and  
various reactions within the biochemical reaction  
cartridge.

Figure 8 is a flow chart of a first treatment  
procedure.

25 Figure 9 is a longitudinal sectional view of  
a part of the chambers shown in Figure 6.

Figure 10 is a longitudinal sectional view of

another part of the chambers shown in Figure 6.

#### DESCRIPTION OF THE PREFERRED EMBODIMENTS

Hereinbelow, the present invention will be  
5 described more specifically with reference to the  
drawings.

Figure 1 is a perspective view of a  
biochemical reaction cartridge in this embodiment.  
Referring to Figure 1, the cartridge has a two-layer  
10 structure including a reaction portion 1 where a  
reaction is effected and a solution storage portion 2  
disposed thereon for storing solutions such as a  
reagent and a cleaning agent.

A body of each of the reaction portion 1 and  
15 the solution storage portion 2 comprises synthetic  
resin, such as polymethyl methacrylate (PMMA),  
acrylonitrile-butadiene-styrene (ABS) copolymer,  
polystyrene, polycarbonate, polyester or polyvinyl  
chloride. In the case where an optical measurement is  
20 required, the material for the body of the reaction  
portion 1 is required to be transparent or  
semitransparent plastic.

At an upper portion of the reaction portion  
1, a specimen port 3 for injecting a specimen such as  
25 blood by a syringe (injector) is disposed and sealed  
up with a rubber cap. On both side surfaces of the  
reaction portion 1, a plurality of nozzle port 4 into

which nozzles are injected to apply or reduce pressure in order to move a solution in the reaction portion 1. A rubber cap is fixed on each of the nozzle ports 4. The other side surface of the reaction portion 1 has a similar structure.

Further, to an upper portion of the solution storage portion 2, 3 aluminum foil sheets are applied for blocking an upper portion of a solution storage chamber described later. The reaction portion 1 and the solution storage portion 2 are bonded to each other through ultrasonic fusion. Incidentally, the reaction portion 1 and the solution storage portion 2 are separately prepared and the solution storage portion 2 may be superposed on the reaction portion 1 at the time of use.

To the side surface of the biochemical reaction cartridge, a bar code label 40 for identifying the type of cartridge is adhered. When the biochemical reaction cartridge is set to a treatment apparatus described later, the bar code is read and the type of the cartridge is identified from the result. Setting of the treatment apparatus is automatically performed so as to effect an appropriate treatment procedure.

Figure 2 is a plan view of the solution storage portion 2 of Figure 1. Referring to Figure 2, the solution storage portion 2 is provided with

independent chambers 6a to 6m each containing a solution. In the chambers 6 and 6b, a first hemolytic agent containing EDTA (ethylenediaminetetraacetic acid) for destructing cell wall and a second hemolytic agent containing a protein modifying agent such as a surfactant are stored, respectively.

In the chamber 6c, particles of magnetic material coated with silica by which DNA is adsorbed are stored. In the chambers 6l and 6m, a first extraction cleaning liquid and a second extraction cleaning liquid, which are used for purifying DNA at the time of extraction of DNA are stored, respectively.

An eluent, comprising a buffer of low concentration salt, for eluting DNA from the magnetic particles, is stored in the chamber 6d, a mixture liquid for PCR (polymerase chain reaction) comprising a primer, polymerase, a dNTP (deoxyribonucleotide triphosphate), a buffer, Cy-3dUTP containing a fluorescent agent, etc., is stored in the chamber 6g. In the chambers 6h and 6j, a cleaning agent containing a surfactant for cleaning a fluorescence-labeled specimen DNA, which is not subjected to hybridization, and a fluorescence label are stored. In the chamber 6i, alcohol for drying the inside of a chamber including a DNA microarray described later is stored. The respective chambers 6a to 6m are provided with a



sharp-pointed valve stems (rods) 7a to 7m,  
respectively, described later, for penetrating the  
sheets.

Figure 3 is a sectional view showing a  
5 storage state in the biochemical reaction cartridge.  
Referring to Figure 3, into the chamber 6, containing  
a solution, of the solution storage portion 2, the  
valve stem 7 provided with a cut 8 is injected and  
supported by two o-rings. The bottom of the solution  
10 chamber 6 is blocked by an aluminum foil sheet 10. A  
sealing member 12 is disposed between the chamber 6  
and the chamber 11 of the reaction portion 1 so as to  
make it impossible for air to enter and exit. Changes  
in volume of solution and air and in pressure due to  
15 environment can be adsorbed by deformation of the  
aluminum foil sheet 10, so that the solution in the  
chamber 6 cannot unexpectedly enter the reaction  
portion 1.

Figure 4 illustrates such a state that after  
20 a tester injects a liquid specimen such as blood from  
the specimen port 3 and sets the biochemical reaction  
cartridge to a treatment apparatus described later, a  
robot arm (not shown) presses the valve stem 7 by  
first-stage pushing with a shorter pressing rod 13a of  
25 a rod needle 13 to stare the aluminum foil sheet, thus  
starting movement of the solution from the chamber 6  
to the chamber 11. In this state, the two O-rings 8

are located in the cut 8 of the valve stem 7, so that the chamber 6 communicates with outside air.

Accordingly, the solution can be moved smoothly.

As described above, the biochemical reaction  
5 cartridge has the penetrable aluminum sheet 10 as a partition member, so that only the pressing the pressing rod 13a of the tool needle 13 toward the reaction portion 1, it is possible to readily cause the solution to flow from the chamber 6 into the  
10 chamber 11 without causing contact of the tool needle 13 with the solution. Incidentally, in this embodiment, immediately under the position of the chamber of the solution storage portion 2, a corresponding chamber of the reaction portion 1 is  
15 located but there is no harm in shifting the corresponding chamber from the position immediately under the chamber of the solution storage portion 2 if, e.g., a passage is provided therebetween.

In this embodiment, the chamber of the  
20 reaction portion 1 and the chamber of the solution storage portion 2 are in a one-to-one relationship but a plurality of solution storage chambers may be provided per one chamber for the reaction portion 1. Further, in this embodiment, the solution is moved  
25 from the solution storage chamber to a blank chamber of the reaction portion 1 but may be moved from the solution storage chamber to a chamber of the reaction

portion 1 already containing a specimen or a solution during treatment. Further, in this embodiment, the aluminum foil sheet 10 is used as the partition member but the partition member per se may be a non-

5 penetrable member if it is provided with an ordinary valve and the valve is placed in a penetrable state, i.e., an open state so as to permit flowing of the solution into the chamber of the reaction portion 1.

Next, the tester once extracts the tool  
10 needle 13 from the treatment apparatus by using the robot arm and turns the tool needle 13 upside down, followed by further pressing the valve stem 7 by second-stage pushing with a longer pressing rod 13b as shown in Figure 5. As a result, air is sealed up by  
15 the upper O-ring 9 to permit movement of the solution in the reaction portion 9 to permit movement of the solution in the reaction portion 1 as described later. The tester performs this step with respect to all the chambers 6a to 6m. As described above, the solution  
20 can be caused to flow into the chamber by the first-stage pushing and the chamber can be sealed up by the second-stage pushing, so that it is possible to effect flowing of the solution into the chamber 11 and sealing of the chamber 11 at the same time only by  
25 simple pushing operations. Further, the above-described tool needle may be provided in the biochemical reaction cartridge.

Figure 6 is a plan view of the reaction portion 1. Referring to Figure 6, on one side surface of the reaction portion 1, 10 nozzle ports 4a to 4j are provided and also on the other side surface thereof, 10 nozzle ports 4k to 4t are provided. The respective nozzle ports 4a to 4t communicate with chambers 11a to 11t, which are portions or sites for storing the solution or causing a reaction, through corresponding air passages 14a to 14t for air flow, respectively.

In this embodiment, however, the nozzle ports 4n, 4p, 4q and 4s are not used, these nozzle ports do not communicate with the chambers and are used as reserve ports. More specifically, in this embodiment, the nozzle ports 4a to 4j communicate with the chambers 11a to 11j through the passages 14a to 14j, respectively. On the other side surface, the nozzle ports 4k, 4l, 4m, 4o, 4r and 4t communicate with the chambers 11k, 11l, 11m, 11o, 11r and 11t through the passages 14k, 14l, 14m, 14o, 14r and 14t, respectively.

The specimen port 3 communicates with a chamber 16. The chambers 11a, 11b, 11c and 11k communicate with the chamber 16, the chambers 11g and 11o communicate with a chamber 17, and the chambers 11h, 11i, 11j, 11r and 11t communicate with a chamber 18. Further, the chamber 16 communicate with the

chamber 17 via a passage 19, and the chamber 17 communicates with the chamber 18 via a passage 20. With the passage 19, the chambers 11d, 11e, 11f, 11l and 11m communicate via passages 15d, 15e, 15f, 15l and 15m, respectively. At a bottom (undersurface) of the chamber 18, a square hole is provided. To the square hole, a DNA microarray 21, on which several tens to several hundreds of thousand of different species of DNA probes are arranged in high density on a surface of solid phase, such as a glass plate having a size of ca. one square centimeter, with the probe surfaces up, is attached.

It is possible to test a large number of genes at the same time by effecting a hybridization reaction with the specimen DNA with the use of the microarray 21.

The DNA probes are regularly arranged in a matrix form, and an address (position determined by the number of row and the number of column on the matrix) of each of the DNA probes is readily read as information. The genes to be tested includes, e.g., genetic polymorphism of each individual in addition to infections viruses, bacteria and disease-associated genes.

In the chambers 11a and 11b of the reaction portion 1, a first hemolytic agent and a second hemolytic agent to be moved from the chambers 6a and

6b, the solution storage portion 2 are stored, respectively. In the chamber 11c, particles of magnetic material to be moved from the chamber 6 are stored. In the chambers 11l and 11m, a first  
5 extraction cleaning liquid and a second extraction cleaning liquid to be moved from the chambers 6l and 6m are stored, respectively. An eluent flowing from the chamber 6d is stored in the chamber 11d, a mixture liquid necessary for PCR (polymerase chain reaction)  
10 moved from the chamber 6g is stored in the chamber 11g. In the chambers 11h and 11j, cleaning agents to be moved from the chambers 6h and 6j are stored, respectively. In the chamber 11i, alcohol to be moved from the chamber 6i is stored.

The chamber 11e is a chamber in which dust  
15 other than DNA of blood accumulates, the chamber 11f is a chamber in which waste of the first and second extraction cleaning liquids in the chambers 11l and 11m accumulates, the chamber 11r is a chamber in which waste of the first and second cleaning agents  
20 accumulates, and the chambers 11k, 11o and 11t are blank chambers provided for preventing the solution to flow into the nozzle ports.

Figure 7 is a schematic view of the treatment apparatus for controlling movement of the solution  
25 within the biochemical reaction cartridge and various reactions.

On a table 22, the biochemical reaction

cartridge is mounted. Further, on the table 22, an  
electromagnet 23 to be actuated at the time of  
extracting DNA or the like from the specimen in the  
cartridge 1, a Peltier element 24 for effecting  
5 temperature control at the time of amplifying DNA from  
the specimen through a method such as PCR (polymerase  
chain reaction), and a Peltier element 25 for  
effecting temperature control at the time of  
performing hybridization between the amplified  
10 specimen DNA and the DNA probe on the DNA microarray  
within the cartridge 1 and at the time of cleaning or  
washing the specimen DNA which is not hybridized, are  
disposed and connected to a control unit 26 for  
controlling the entire treatment apparatus. Further,  
15 the robot arm (not shown) for pushing down the valve  
stem by moving the tool needle 13 above a  
predetermined chamber on the cartridge as described  
above, and a bar code reader (not shown) for reading  
the bar code label applied to the cartridge are  
20 provided to the treatment apparatus.

At both side surfaces of the table 22, an  
electric (motor-driven) syringe pumps 27 and 28 and  
pump blocks 31 and 32 each of which is a port for  
discharging or sucking in air by these pumps 27 and 28  
25 and is provided with 10 pump nozzles 29 or 30 on its  
side surface, are disposed. Between the electric  
syringe pumps 27 and 28 and the pump nozzles 29 and

30, a plurality of known electric switching (selector) valves (not shown) are disposed and connected to the control unit 26 together with the pumps 27 and 28. The control unit 26 is connected to an input unit 33  
5 to which inputting by a tester is performed. The control unit 26 controls the pump nozzles 29 and 30 so that each of the respective 10 pump nozzles is selectively opened and closed with respect to the electric syringe pumps 27 and 28, respectively.

10 When the solution is moved from the solution storage portion 2 to the reaction portion 1 and a treatment start signal is inputted, extraction and amplification of DNA or the like are performed within the reaction portion 1. Further, hybridization  
15 between the amplified specimen DNA and DNA probes on the DNA microarray disposed in the reaction portion 1 and cleaning of the fluorescence-labeled specimen DNA, which is not hybridized, and the fluorescence label are performed.

20 In this embodiment, when the tester injects blood as a specimen into the reaction portion through the rubber cap of the specimen port 3 by a syringe or an injector, the blood flows into the chamber 16. Thereafter, the tester places the biochemical reaction  
25 cartridge on the table 22 and moves the pump blocks 31 and 32 in directions of arrows indicated in Figure 7 with a mechanism (not shown) by operating an unshown



lever, whereby the pump nozzles 29 and 30 are injected into the corresponding nozzle ports 4 of the reaction portion 1.

As described with reference to Figure 6, the  
5 nozzle ports 4 are concentrated at two surfaces, i.e., both side surfaces, of the biochemical reaction cartridge, so that it is possible to simplify shapes and arrangements of the electric syringe pumps 27 and 28, the electric switching valves, the pump blocks 31  
10 and 32 containing the pump nozzles 29 and 30, etc. Further, by effecting such a simple operation that the cartridge is sandwiched between the pump blocks 31 and 32 at the same time while ensuring necessary chambers and passages, it is possible to inject the pump  
15 nozzles 29 and 30 and simplify the structure of the pump blocks 31 and 32. Further, all the nozzle ports 4a to 4t are disposed at an identical level, i.e., are arranged linearly, whereby all the heights of the passages 14a to 14t connected to the nozzle ports 4a  
20 to 4t become equal to each other. As a result, preparation of the passages 14a to 14t becomes easy.

Further, in the treatment apparatus shown in Figure 7, in the case where the length of the pump blocks 31 and 32 is increased n times the original  
25 length with respect to n biochemical reaction cartridges, when the n cartridge are arranged in series, it is possible to perform a necessary step to

all the n cartridges at the same time. As a result, a biochemical reaction can be performed in the large number of biochemical reaction cartridges with a very simple apparatus structure.

5               When the tester performs the steps of flowing of the solution into the chamber and hermetically sealing the chamber described with reference to Figures 4 and 5 and then inputs a treatment start instruction at the input unit 33, the bar code label  
10   applied to the biochemical reaction cartridge is first read by the bar code reader (not shown) of the treatment apparatus. In the treatment apparatus, treatment sequences necessary for the respective types of cartridges are memorized in advance. When the type  
15   of cartridge is identified by the read bar code, the contents and procedures of treatment necessary for the cartridge are automatically determined to start the treatment. When the bar code cannot be read or the read bar code is not a predetermined bar code, the  
20   tester can also manually input treatment steps by the input unit 33.

              Figure 8 (consisting of Figures 8A and 8B) is a flow chart for explaining an example of a treatment procedure in the treatment apparatus in this  
25   embodiment.

              Referring to Figure 8, in a step S1, the first hemolytic agent is moved from the solution

storage chamber 6a to the chamber 11a of the reaction  
portion 1 by effecting injection of the solution and  
hermetic sealing as described with reference to  
Figures 4 and 5. In a step S2, the control unit 26  
5 opens only the nozzle ports 4a and 4b, and air is  
discharged from the electric syringe pump 27 and  
sucked in the reaction portion 1 from the electric  
syringe pump 28, whereby the first hemolytic agent is  
injected from the chamber 11a into the chamber 16  
10 containing blood. At this time, by controlling  
suction of air from the pump 28 so as to start 10 -  
200 msec after initiation of air discharge from the  
pump 27, the solution can flow smoothly without  
causing splash or scattering thereof at its leading  
15 end although it depends on a viscosity of the  
hemolytic agent and a resistance of the passage.

As described above, by shifting timing of  
supply and suction of air so as to control a manner of  
pressure application and pressure reduction, it is  
20 possible to cause the solution to flow smoothly. In a  
preferred embodiment, the solution can be caused to  
flow further smoothly by effecting such a control that  
a degree of suction of air from the electric syringe  
pump 28 is linearly increased from the initiation of  
25 air discharge from the pump 27. Further, it becomes  
possible to alleviate the pressure generated in the  
reaction portion 1 by applying and reducing pressure

in combination. As a result, it is also possible to achieve such an effect that the solution is prevented from flowing into a branched passage or chamber in the case where the solution is not intended to flow into the branched passage or chamber during movement thereof. These are true in the case of subsequent liquid movement.

The air supply control can be readily realized by using the electric syringe pumps 27 and 28. More specifically, after only the nozzle ports 4a and 4o are opened, discharge and suction of air are repeated alternately by the syringe pumps 27 and 28 to cause repetitive flow and flowback of the solution of the chamber 6 in the passage 19, thus stirring the solution. Alternatively, the solution can be stirred while continuously discharging air from the pump 28 to generate bubbles.

Figure 9 is a sectional view of the reaction portion 1 shown in Figure 6 along a cross section intersecting the chambers 11a, 16 and 11k, and shows such a state that the nozzle port 4a is pressurized by injecting therein the pump nozzle 29 and the nozzle port 4k is reduced in pressure by injecting therein the pump nozzle 30, whereby the first hemolytic agent in the chamber 11a flows into the chamber 16 containing blood.

Referring again to Figure 8, in a step S4,

only the nozzle ports 4b and 4k are opened and the second hemolytic agent in the chamber 11b is caused to flow into the chamber 16 in the same manner as in the case of the first hemolytic agent. Similarly, in a  
5 step S5, the magnetic particles in the chamber 11, after being moved from the chamber 6c to the chamber 11, are caused to flow into the chamber 16. In the steps S4 and S6, stirring is performed in the same manner as in the step S2. In the step S6, DNA  
10 resulting from dissolution of cells in the steps S2 and S4 attaches to the magnetic particles.

Thereafter, in a step S7, an electromagnet 23 is turned on and only the nozzle ports 4e and 4k are opened. Then, air is discharged from the electric  
15 syringe pump 28 and sucked in from the pump 27 to move the solution from the chamber 16 to the chamber 11e. At the time of movement, the magnetic particles and DNA are trapped in the passage 19 on the electromagnet 23. The suction and discharge by the pumps 27 and 28  
20 are alternately repeated to reciprocate the solution two times between the chambers 16 and 11e, whereby a trapping efficiency of DNA is improved. The trapping efficiency can be further improved by increasing the number of reciprocation. In this case, however, it  
25 takes a longer treating time by that much.

As described above, DNA is trapped in a flowing state on such a small passage having a width

of about 1 - 2 mm and a height of about 0.2 - 1 mm by utilizing the magnetic particles, so that DNA can be trapped with high efficiency. This is also true for RNA and protein.

5           Then, in a step S8, the electromagnet 23 is turned off, and only the nozzle ports 4f and 4l are opened. Thereafter, air is discharged from the electric syringe pump 28 and sucked in from the pump 27 to move the first extraction cleaning liquid from  
10 the chamber 11l to the chamber 11f. At this time, the magnetic particles and DNA trapped in the step S7 are moved together with the extraction cleaning liquid, whereby cleaning is performed. After the reciprocation of two times is performed in the same  
15 manner as in the step S7, the electromagnet 23 is turned on, and the reciprocation of two times is similarly performed to recover the magnetic particles and DNA in the passage 19 on the electromagnet 23 and return the solution to the chamber 11l.

20           In a step S11, cleaning is further performed in the same manner as in the step S5 by using the second extraction cleaning liquid in the chamber 11m, after being moved from the chamber 6m to the chamber 11m in a step S10, in combination with the nozzle  
25 ports 4f and 4m.

          In a step 12, the eluent is moved from the chamber 6d to the chamber 11d. In a step S13, only

the nozzle ports 4d and 4o are opened while the  
electromagnet 23 is kept on, and air is discharged  
from the pump 27 and sucked in from the pump 28,  
whereby the eluent in the chamber 11d is moved to the  
5 chamber 17.

At this time, the magnetic particles and DNA  
are separated by the action of the eluent, so that  
only the DNA is moved together with the eluent to the  
chamber 17, and the magnetic particles remain in the  
10 passage 19. Thus, extraction and purification of the  
DNA are performed. As described above, the chambers  
11l and 11m containing the extraction cleaning liquids  
and the chamber 11f containing waste liquid after the  
cleaning are separately provided, so that it becomes  
15 possible to effect extraction and purification of the  
DNA in the biochemical reaction cartridge.

Next, in a step S14, the PCR agent is moved  
from the chamber 6g to the chamber 11g. In a step  
S15, only the nozzle ports 4g and 4o are opened, and  
20 air is discharged from the electric syringe pump 27 and  
sucked in from the pump 28 to cause the PCR agent in  
the chamber 11g to flow into the chamber 17. Further,  
only the nozzle ports 4g and 4t are opened, and air  
discharge and suction by the pumps 27 and 28  
25 are repeated alternately to cause the solution in the  
chamber 16 to flow into the passage 20. Thereafter,  
the returning operation is repeated to effect

stirring. Then, the Peltier element 24 is controlled to retain the solution in the chamber 17 at 96 °C for 10 min. Thereafter, a cycle of heating at 96 °C/10 sec, 55 °C/10 sec, and 72 °C/1 min. is repeated 30  
5 times, thus subjecting the eluted DNA to PCR to amplify the DNA.

In a step S16, only the nozzle ports 4g and 4t are opened, and air is discharged from the electric syringe pump 27 and sucked in from the pump 28 to move  
10 the solution in the chamber 17 to the chamber 18. Further, by controlling the Peltier element 25, the solution in the chamber 18 is kept at 45 °C for 2 hours to effect hybridization. At this time, discharge and suction of air by the pumps 27 and 28  
15 are repeated alternately to move the solution in the chamber 18 to the passage 15t. Thereafter, the hybridization proceeds while effecting stirring by repeating the returning operation.

Then, after the first cleaning liquid is  
20 moved from the chamber 6h to the chamber 11h in a step S17, in a step S18, while keeping the temperature at 45 °C, only the nozzle ports 4h and 4r are opened, and air is discharged from the electric syringe pump 27 and sucked in from the pump 28 to cause the first  
25 cleaning liquid in the chamber 11h to flow into the chamber 11r through the chamber 18 while moving the solution in the chamber 18 to the chamber 11r. The



suction and discharge by the pumps 27 and 28 are repeated alternately to reciprocate the solution two times between the chambers 11h, 18 and 11r and finally return the solution to the chamber 11h. Thus, the  
5 fluorescence-labeled specimen DNA and the fluorescence label which are not hybridized are cleaned.

Figure 10 is a sectional view of the reaction portion 1 shown in Figure 6 along a cross section intersecting the chambers 11h, 18 and 11r. The  
10 reaction portion 1 is pressurized by injecting the pump nozzle 29 into the nozzle port 4h and is reduced in pressure by injecting the pump nozzle 30 into the nozzle port 4r. Figure 10 illustrates such a state that the first cleaning liquid is caused to flow into  
15 the chamber 11r through the chamber 18. The chamber 11h actually communicates with the solution storage portion 2 but in Figure 10, is illustrated as a state in which it does not communicate with the solution storage portion 2 by providing a ceiling thereof, for  
20 convenience of explanation.

Referring again to Figure 8, after the second cleaning liquid is moved from the chamber 6j to the chamber 11j in a step S19, in a step S20, while keeping the temperature at 45 °C, the cleaning is  
25 further effected in the same manner as in the step S10 by using the second cleaning liquid in the chamber 11j in combination with the nozzle ports 4j and 4r, and

the solution is finally returned to the chamber 11j.  
As described above, the chambers 11h and 11j  
containing the cleaning liquids and the chamber 11r  
containing waste liquid after the cleaning are  
5 separately provided, so that it becomes possible to  
effect extraction and purification of the DNA  
microarray 21 in the biochemical reaction cartridge.

After alcohol is moved from the chamber 6i to  
the chamber 11i in a step S21, in a step 22, only the  
10 nozzle ports 4i and 4r are opened, and air is  
discharged from the electric syringe pump 27 and  
sucked in from the pump 28 to move alcohol in the  
chamber 11i to the chamber 11r through the chamber 18.  
Thereafter, only the nozzle port 4i and 4t are opened,  
15 and air is discharged from the pump 27 and sucked in  
from the pump 28 to dry the inside of chamber 18.

Thereafter, when the tester operates a lever  
(not shown), the pump blocks 31 and 32 are moved away  
from the biochemical reaction cartridge. As a result,  
20 the pump nozzles 29 and 30 are removed from the nozzle  
ports 4 of the cartridge. Then, the tester mounts the  
cartridge in a reader for DNA microarray, such a known  
scanner to effect measurement and analysis.

In the above-described embodiment, the  
25 identification of the cartridge is performed by using  
the bar code label but may also be performed by using  
a two-dimensional bar code, an IC chip, PFID (radio

frequency identification), etc. Further, on the basis of external dimensions of the cartridge such as height and length, the number of recesses or projections provided on the side surfaces, the upper surface and  
5 the lower surface of the cartridge, and a combination thereof, the type of the cartridge can be identified in various manners. As a result, it is possible to attain a similar effect.

In the above embodiment, the identification  
10 of the cartridge is performed and based on the identified type of the cartridge, treatment steps are set. However, it is also possible to set a treatment sequence on the basis of information, on the contents and procedures of treatment steps, which are written  
15 in the two-dimensional bar code or the like. Further, in the case of changing testing conditions such as a reaction time cartridge by cartridge, different treatment steps are written in a two-dimensional bar code and the bar code is adhered to the cartridge,  
20 whereby it becomes possible to effect a desired reaction step with reliability.

As described hereinabove, the biochemical reaction cartridge according to the present invention has a reaction portion including a chamber and a  
25 passage and a solution storage portion, which is isolated or separated from the reaction portion, for storing a solution such as a reagent or a cleaning

agent, and is constituted by such a member that it is separated for moving the solution from the solution storage portion to the reaction portion and is penetrable or that it is a penetrable member disposed  
5 at a boundary wall portion between the solution storage portion and the reaction portion which contact each other. As a result, respective solutions can be prepared with the biochemical reaction cartridge immediately before the respective treatment steps, so  
10 that the biochemical reaction cartridge has the advantage of causing an intended reaction properly without causing a reagent in a chamber to flow into a passage or another chamber even when an environmental change or vibration occurs during a treatment step  
15 using another solution.

Further, particularly, a step of moving each of the solutions in the solution storage portion to the reaction portion immediately before use the solution is employed, so that it is possible to effect  
20 reliable reaction without causing the solution to flow into adjacent chambers and passages even when vibration of the treatment apparatus occurs or there arises an error of pressure control during treatment in each of the steps.

25 Further, the treatment apparatus automatically reads the bar code label applied to the biochemical reaction cartridge and identifies the type

of the cartridge, thus automatically setting necessary treatment steps. Accordingly, it becomes possible to simply effect the treatment with reliability since it is not necessary for the operation to set a  
5 complicated treatment procedure on all such occasions that there are a plurality of cartridge types.

Further, since the biochemical reaction cartridge of the present invention has the above-described structure, it is possible to prepare a  
10 solution therein as desired. As a result, the biochemical reaction cartridge eliminates the inconvenience of replenishing a reagent and reduces an error in selection of the type of reagent. In addition, even when an environmental change or  
15 vibration is caused to occur at the time of storage and conveyance, the reagent in the chamber does not flow into a passage or another chamber. Accordingly, the biochemical reaction cartridge can cause an intended reaction appropriately.

20 While the invention has been described with reference to the structures disclosed herein, it is not confined to the details set forth and this application is intended to cover such modifications or changes as may come within the purposes of the  
25 improvements or the scope of the following claims.